

A New Wavelet-based Algorithm for R-peak Detection in ECG and it's a Comparison with the Currently Existing Algorithms

M. S. Dahwah

Ph.D. student at Applied Mathematics and Informatics Department
Mari State University
Yoshkar-Ola, Russia

A. N. Leukhin

Professor at Applied Mathematics and Informatics Department
Mari State University
Yoshkar-Ola, Russia

ABSTRACT

The purpose of this paper is to develop a new approach for R-peak detection in ECG and compare it with the most effective and existing algorithms. The proposed approach is based on DWT and envelope for the first stage of preprocessing and decision or detecting it was achieved by adaptive thresholding. The proposed algorithm is compared with Pan & Tompkins, Savitzky-Golay smoothing filter, Hilbert and wavelet transforms as well as fast Fourier transform algorithm to investigate these techniques of R peak detection and evaluate the wavelet-based algorithm comparing with them. The algorithms are evaluated in the experimental section using ECG signals from the MIT-BIH database. The results of detection algorithms show that the proposed wavelet-based algorithm gets the highest sensitivity by 99.9% with higher reliability compared to other algorithms, also by analyzing the precision of them, it's come to light that FFT improved the highest precision with 99.7%.

Keywords

ECG, Pan & Tompkins, Savitzky-Golay smoothing filter, Fast Fourier transform, wavelet transforms, Hilbert transform, R peak.

1. INTRODUCTION

One of the most popular bio-signals in the biomedical engineering is electrocardiography, and R peak is the most important part of ECG signal because of it's an essential role in detection, segmentation and feature extraction in ECG and also in determining heart rate variability.

The detection of peaks and feature extraction in bio-signals are an important step in many processing and classification applications, so it is very important to have an accurate algorithm for detecting this peaks in several signals such ECG shown in Fig.1, as well as determine the exact time when it appears, and this will be possible by reducing noise as an initial step to be able for a high probability of correct detection [1,2].

The preprocessing of ECG signal involves removing of baseline wanders and power line interference. Baseline wander is usually ranged between 0.5 Hz up to 0.75 Hz during the contraction of muscles. A diverse source of noise is because of the electromagnetic fields by the power line with the frequency of 50 Hz (60 Hz in some countries, i.e. US and Japan). Types of different noises make the detection of ECG peaks more complicated as the low amplitude waveforms become unreliable and spurious waveforms may be introduced [3].

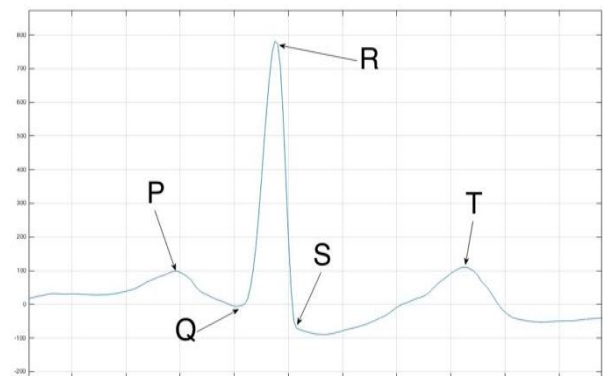


Fig 1: Sample ECG from MIT-BIH Database

The researchers, over the last 20 years, shows that the suggested algorithms in this paper for ECG analysis and specifically for peaks detection based on several signal processing techniques have reached a reliable detection performance [4].

In the field of ECG processing various algorithms have been reported specifically for the QRS complex such:

- Differentiation algorithms [2]
- Digital filters [5-9]
- Neural networks [10-12]

In fact, most of the presented algorithms have a fundamental problem known as sensitivity to noise [13]. The problem of sensitivity to noise in ECG signal in itself is complex and because of that, in this paper, it is chosen six algorithms for preprocessing the electrocardiography in order to reduce noise before detecting R wave. This paper aims to get benefits from the advantages of Pan & Tompkins algorithm, Savitzky-Golay smoothing filter, Hilbert and wavelet transform as well as fast Fourier transform in order to approach an optimum algorithm for R peak detection.

2. MATERIALS AND ALGORITHMS

In most peaks detection algorithms there are two varied stages, the first one is preprocessing and the second it will be the decision. In the preprocessing stage, different techniques are applied to the signal, six of these approaches were applied to ECG signal in this work. For better evaluation of the algorithms, they are tested on ECG signals selected from the MIT-BIH database with 9000 samples and results will be related to each algorithm that will be shown separately in each algorithm sections.

2.1 Pan & Tompkins

In this section, has been employed Pan & Tompkins algorithm. This algorithm is based on passing ECG signal successively through some processes which based on band-pass filter, differentiator and squaring[14]. The band-pass filtering removes baseline wander and the high-frequency noise from the original ECG signal [15]. The differentiator preserves the information about the QRS complex slopes [16]. ECG squaring helps to emphasize the differences between the QRS complex with P and T waves [17].

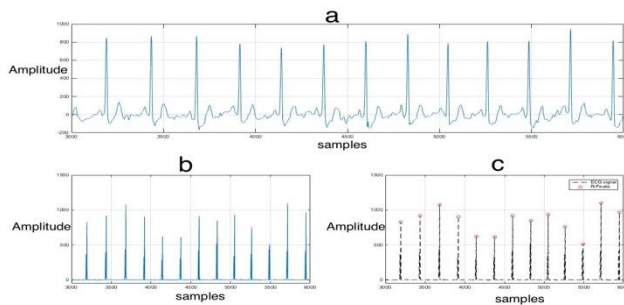


Fig 2: Sample ECG data, (a) original ECG, (b) processed ECG, (c) R detected in ECG signal

Original ECG is shown in Figure 2 (a), in order to attenuate noise the ECG signal passes through a digital band-pass filter composed of cascaded high and low pass filters, the output of this filter after the differentiation and squaring shown in (b), the final signal with the detected R peaks are presented in (c).

2.2 Savitzky-Golay smoothing filter

The main purpose of the Savitzky-Golay filter is to smooth the data, such filters are also named least squares or digital smoothing polynomial filters. In this section, smoothing ECG signal and then adaptive thresholding technique for R wave detection it was applied. According to Table 1, the algorithm which introduced is based on using three general stages including Savitzky-Golay filter, squaring and adaptive thresholding. Fig.3 shows ECG signals at various steps in signal processing by S-GSF algorithm.

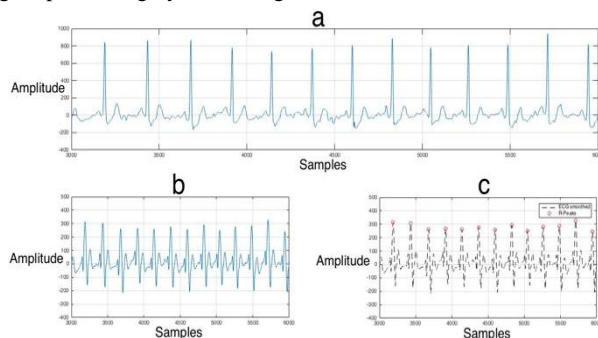


Fig 3: Sample ECG data (a), Original ECG: (b), processed ECG: (c), R detected in ECG signal

2.3 Wavelet transform

The ability of the wavelet transform is tested in different works of peaks detection [18-20]. In this section, has been applied algorithm based on wavelet transform, is proposed for noise reduction and R peak detection. According to Table 1, WT algorithm has appeared a low probability of correct detection as well as the probability of false detection. The algorithm introduced in this section is based on two general stages: WT and adaptive thresholding. Figure 4 shows ECG signals at various steps in signal processing by WT algorithm.

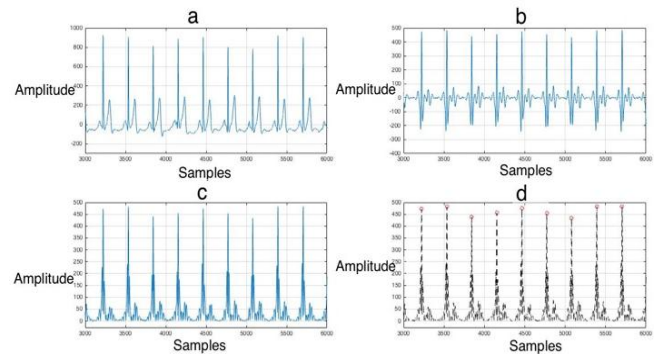


Fig 4: Sample ECG data, (a) Original ECG, (b) Reconstructed ECG, (c) abs Reconstructed ECG detection, (d) R detected in ECG signal

2.4 Hilbert transform

Peak detection is one of the applications of the Hilbert transform using its properties. The algorithm uses ECG Hilbert transformed data in which undesirable peaks such as T and P waves are maximum minimized which makes R peak detection easily with the presence of various noises. According to Table 1, the algorithm introduced in this section is based on using two general stages including Hilbert transform and adaptive thresholding as shown in Fig.5.

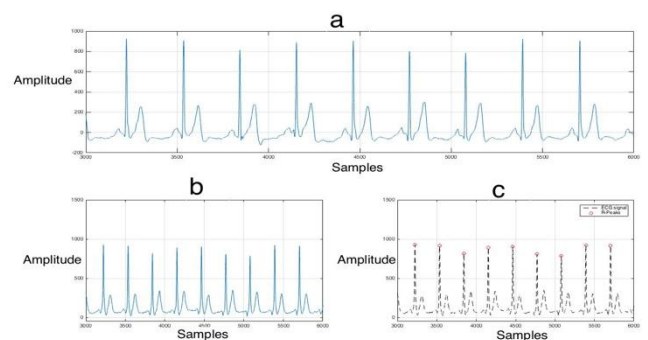


Fig 5: Sample ECG data, (a) Original ECG, (b) Filtered ECG, (c) R peaks detection

2.5 Fast Fourier Transform

The main idea of this algorithm is to apply direct fast Fourier transform, remove low frequencies and restore ECG with the help of inverse fast Fourier transform and then adaptive thresholding technique for R wave detection.

The noisy ECG is shown in Figure 6 (a), after removing the low frequencies from the signal, the output of this step shown in (b), the final signal with the detected R peaks are presented in (c).

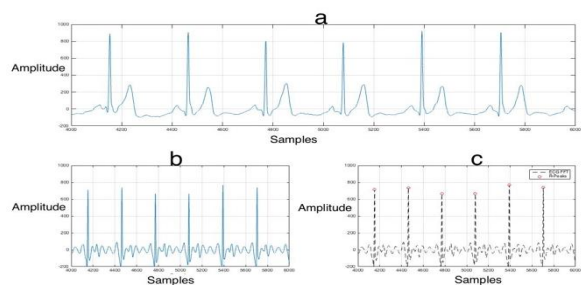


Fig 6: Sample ECG data, (a) Original ECG, (b) Filtered ECG, (c) R detected in ECG signal

2.6 A new wavelet-based algorithm

In this work, it was developed an algorithm for detection R peaks of ECG signals. It reliably detects R peaks based upon DWT and envelope for the first stage of preprocessing and decision or detecting it was achieved by adaptive thresholding. The wavelet transform can be used as a signal decomposition in the plane of the time scale. There are many applications of wavelet transforms, such as compression of sub-band encoding data, detection of characteristic points, and noise cancellation. To reduce the noise of the ECG signal, many algorithms are available, such as digital filters FIR or IIR, adaptive algorithm, and wavelet transformation thresholding algorithms [21].

The wavelet transform describes a decomposition process with several resolutions in terms of a signal extension to a set of wavelet-basis functions. The wavelet has its excellent spatial frequency localization property. The use of DWT in a 1D signal corresponds to a 1D filter in each measurement [22]. The threshold value is used in the frequency domain to smooth out or to remove certain coefficients of the wavelet signal sub-signals of the measured signal. The noise scale in the signal is effectively reduced in a non-stationary environment. The algorithm of noise reduction, which applies a threshold value in the frequency domain, is proposed by Donoho [23].

The introduced algorithm is about decomposition and reconstruction the ECG signal into five scales of wavelets by using Daubechies family and getting a threshold value where where the error level is minimized between the thresholded noisy and the original signal.

The algorithm can be sequenced into this steps: 1) Decomposing of signals using wavelet transform: The signals are decomposed into five levels by discrete wavelet transform using wavelet (db4); 2) Choosing threshold value; 3) Reconstruction: The signal is reconstructed using the IDWT [21]. After DW reconstruction of ECG, the signal is squared point by point. This makes all data points positive and does nonlinear amplification of the output of the ECG signal. After that, the peak detector is used to find the peaks in the ECG signal envelope by adaptive thresholding.

Fig.7 shows signals at various steps in digital signal processing (a) show the original ECG. In order to attenuate noise, the ECG signal was decomposed and reconstructed in (b) after that squaring the ECG signal is presented in (c) also (d) shows ECG signal envelope as (e) shows the final signal with R peak detected.

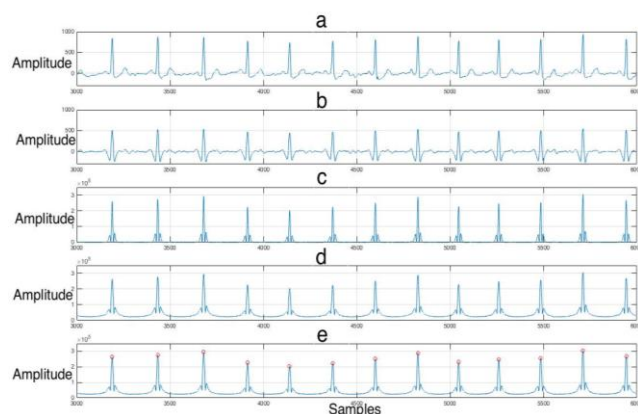


Fig 7: The steps of the wavelet-based algorithm in ECG processing and R detection

3. EVALUATION AND COMPARISON

The evaluation of the performance of the algorithms. Depends on two parameters which should be used to evaluate the detection performance; that is,

$$TPR=TP/P \quad \text{sensitivity} \quad (1)$$

$$PPV=TP/TP+FP \quad \text{precision} \quad (2)$$

where TP denotes the number of true positive detections, P positive samples, and FP the number of false positives. Furthermore, to achieve comparable and reproducible results, the evaluation needs to be carried out on standard databases which are MIT-BIH in this research. Variety of R peak detection algorithms presented in table 1 reflects the need for a reliable R peak detection in ECG processing. Sensitivities of about 99.9% are possible for R peak detectors as shown in table 1.

Table 1. Statistical results for the algorithms

	Algorithm	QRS detection sequence	Efficiency	TPR	PPV
1	Pan And Tompkins	First derivative + squaring + band-pass filter + adaptive thresholding	Medium	98.9	98.2
2	Savitzky-Golay smoothing filter	Savitsky-Golay filter +squaring +adaptive thresholding	Low	95.8	97.7
3	Wavelet transform	WT+ adaptive thresholding	Low	95.9	97.4
4	Hilbert transform	Hilbert transform + adaptive thresholding	Low	97,5	96.7
5	Fast Fourier transform	FFT/IFFT+ adaptive thresholding	Low	97.2	99.7
6	A new-wavelet based algorithm	Wavelet decompose and reconstruction, + squaring+ envelope, + adaptive thresholding	High	99.9	99.3

4. RESULTS AND DISCUSSION

About 725 beats from the MIT-BIH Arrhythmia database, without exception, were used for evaluating the algorithms. The results are presented in Table 1. Two parameters were used to evaluate the algorithms for each signal; that is, sensitivity and precision. From the chart and Table 1 it's come to light that a new wavelet-based algorithm improved the highest sensitivity by 99.9%, with precision by 99.3% as shown in fig.8. The evaluation data of all algorithms presented in this work in Table 1 are shown as a chart in Fig.8.

R peak is detected using a new wavelet-based algorithm with high reliability. These detection rates may be sufficient for diagnostic applications in cardiac therapy, as well as a higher performance may be necessary for research purposes also.

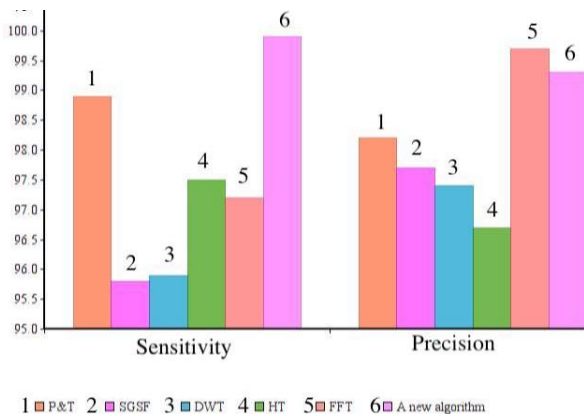


Fig 8: A chart of the evaluation data of all R detection algorithms

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